Cosilencing of PKM-2 and MDR-1 Sensitizes Multidrug-Resistant Ovarian Cancer Cells to Paclitaxel in a Murine Model of Ovarian Cancer

Meghna Talekar1, Qijun Ouyang1, Michael S. Goldberg2, and Mansoor M. Amiji1

Introduction

Ovarian cancer is one of the most common female gynecological malignancies and has an average 5-year survival rate of 44% (1). Because the majority of patients present with advanced stages of the disease, monotherapies typically do not confer meaningful efficacy. As a result, innovative strategies to prolong disease remission are being explored. Paclitaxel is a standard treatment for ovarian cancer, though its effectiveness often diminishes over the course of treatment owing to the emergence of multidrug resistance (MDR). MDR develops as a consequence of several factors, including poor systemic drug delivery due to vascular abnormalities, insufficient intracellular availability, and microenvironmental selection pressures (2). Among these, one of the most studied resistance mechanisms is the reduction in intracellular drug concentration by efflux transporter proteins that pump drugs out of cells. Many of these transporters are members of the ATP-binding cassette transmembrane protein super-family, including P-glycoprotein (P-gp) and MDR protein-1 (MRP-1). Although increasing the dosing of anticancer agents can transiently increase intracellular drug concentrations, dose-limiting toxicities can necessitate drug-free recovery periods that lead to reversion to MDR.

Along with drug resistance, cancer cells also undergo adaptations in cellular respiration to enhance their tumorigenic and metastatic potential (3). Cellular respiration is a series of catabolic reactions that yield ATP. In healthy cells, this occurs by the energy-efficient oxidative phosphorylation (OXPHOS) system (yielding between 30 and 36 ATPs for every glucose molecule), whereas cancer cells show a propensity to rely on a less energy-efficient process termed aerobic glycolysis (which yields two ATPs for every glucose molecule) for energy. Although this dependence of cancer cells on aerobic glycolysis would seem detrimental energetically, cancer cells are not limited for ATP and prioritize conversion of glucose to biomass for dividing cells. From a therapeutic perspective, these metabolic differences between cancer cells and healthy cells can be used to discriminate these cell types, thereby avoiding the harsh side effects of cytotoxic therapies.

Pyruvate kinase (PK) is a critical enzyme in the glycolysis pathway that has been avidly explored as a potential target for cancer therapy. It catalyzes the final irreversible rate-limiting step of glycolysis by dephosphorylating phosphoenolpyruvate (PEP) into pyruvate and produces one molecule of ATP in the process. PK has 4 isoforms (L, R, M1, and M2) with a specific...
tissue distribution pattern (4). PKM-1 and PKM-2 are different splicing products of the same mRNA transcribed from the PKM gene. The PKM-1 isomorph is expressed in energy-intensive organs such as muscles, brain, heart, and kidney, whereas PKM-2 is expressed in lungs, fat, pancreatic islets, and in cells with a high rate of nucleic acid synthesis, such as embryonic cells, adult stem cells, and tumor cells. Because of a high expression in tumor cells, novel inhibitors (5, 6) and nucleic acid therapies (7–9) have been designed to target PKM-2 to achieve anticancer activity.

RNA interference (RNAi) is a biological process in which RNA molecules (miRNA or siRNA) inhibit gene expression, typically by causing the destruction of complementary mRNA molecules. It has emerged as a powerful strategy for cancer therapy, especially MDR cancer. Frustratingly, delivery of these therapies to specific tumor tissues and cells followed by intracellular release from endosomal/lysosomal compartments into the cytoplasm still remains a major hurdle. Naked RNAi-based therapy is unfavorable because of the charge, size, and instability of siRNAs. Although viral vectors are efficient tools for gene delivery, concerns regarding their toxicity have limited their clinical applications, necessitating development of safer alternatives. Nonviral/polymeric nanoparticle (NP)–based delivery platforms are becoming viable alternatives for delivery of RNAi-based therapies. Indeed, siRNA against PKM-2 has been successfully delivered by NPs to induce cell apoptosis and tumor regression (7, 10). Goldberg and colleagues had previously reported the delivery of M2 isoform-specific siPKM2 in lipidoid formulations in HepG2 and SKOV-3 tumor bearing mice. The siRNA NPs showed a 76% and 85% decrease in tumor volume relative to the controls (7).

In our experience, encapsulation of siMDR-1 and paclitaxel in polymeric NPs has provided MDR-1 gene silencing and subsequent enhancement in cytotoxicity attributed to an increase in intracellular drug concentration in SKOV-3TR cells (11). Similarly, use of lipid functionalized dextran doxorubicin NPs has shown 5- to 10-fold higher antiproliferative activity in drug-sensitive and drug-resistant osteosarcoma (KHO5) and ovarian cancer (SKOV-3) cells lines (12). Recently, we have also assessed the delivery of MDR-1 siRNA to ovarian cancer cells followed by paclitaxel treatment to induce inhibition of tumor growth, decreased P-gp expression, and increased apoptosis (13, 14).

To our knowledge, this is the first report of the combination of an siRNA that directly induces apoptosis and an siRNA that mitigates against chemotherapy efflux prior to cytotoxic chemotherapy. Herein, we describe the dramatically improved efficacy of this combination relative to either siRNA monotherapy prior to cytotoxic chemotherapy in a two MDR models of ovarian cancer. In addition to the combination therapeutic approach, we explored the targeting capability of our hyaluronic acid (HA)–based self-assembling systems by adding targeting moieties to epidermal growth factor receptors, which are highly expressed on ovarian cancer cells (15). To explore this combination therapy in a model that would maximally recapitulate the biology of MDR ovarian cancer, we also developed and assessed our therapies in an in vivo–induced paclitaxel-resistant model. Our data again confirmed the synergistic potential of combination RNAi and cytotoxic therapy for MDR ovarian cancer.

**Materials and Methods**

**Materials**

Sodium hyaluronate (HA) with an average molecular weight of 20 kDa was obtained from Lifecore Biomedical Co. Poly(ethylene imine; PEI MW = 20,000 Da) was obtained from Polysciences Inc. Monofunctional poly(ethylene glycol)–amine (PEG2K–NH2, MW = 2,000 Da) was purchased from Creative PEG Works, Inc. Paclitaxel was purchased from Fisher Scientific.

**Cell lines**

Human ovarian adenocarcinoma cell line SKOV-3 was obtained from ATCC. A paclitaxel-resistant version of this cell line (SKOV-3TR) was obtained from Massachusetts General Hospital (Boston, MA). The cells were cultured in RPMI-1640 medium supplemented with 10% FBS and grown at 37° C, 5% CO2. SKOV-3TR cells were cultured in 20 nmol/L paclitaxel to maintain their drug-resistant phenotype. The resistant phenotype of these cells was regularly assessed by cytotoxicity analysis to determine IC50 values.

**Formation and characterization of siRNA-loaded HA NPs: determination of size, charge, morphology, siRNA encapsulation, and siRNA release**

We have previously published information regarding preparing combinatorial designed HA formulation (16). The HA-PEI and HA-PEG conjugates were prepared using this combinatorial approach (16). For the synthesis of HA-PEG-EG, 50 mg of maleimide-PEG-amine was added to EDC/NHS activated HA. Following synthesis of HA-PEG-maleimide, an EGFR-specific peptide, YHWYGTPQNV designated as GE11 was used for conjugation with maleimide. The GE11 peptide was originally synthesized and screened as an EGFR-specific peptide by Li and colleagues (17). For this study, the GE11 peptide with a spacer sequence of GGGGC was synthesized at Tufts University Core Facility (Boston, MA). We have previously successfully prepared EGFR-targeted polymeric NPs using this peptide sequence (18). The carboxyl group of terminal cysteine of the peptide was reacted with the maleimide of maleimide-PEG-HA in HEPES buffer (pH 7.4) at 1:1 molar ratio while mixing under N2 at 4°C for 24 hours. The peptide conjugate was then purified by dialysis (3.5 kDa), lyophilized, and characterized by nuclear magnetic resonance spectroscopy. Similarly, for the preparation of HA-rhodamine 123, 50 mg of rhodamine 123 was added to the EDC/NHS activated HA, the solution stirred overnight, dialyzed, and lyophilized.

The HA-PEI, HA-PEG solutions (3 mg/mL) were prepared by dissolving the polymer in PBS. NP size and charge were determined on a Malvern Nano ZS (Malvern Instruments). Transmission electron microscopy (JEOL, JEM-1000) was performed to assess the formation of siRNA-loaded NPs. Uranyl acetate ribonucleic acid stain was used to demarcate siRNA from the polymer. The dark staining of siRNA by heavy metals such as uranyl acetate provides a high contrast compared with HA polymer that can help to confirm loading of siRNA in the polymeric NPs. The ability of these complexes to release siRNA was determined by treating them with poly(acrylic acid; PAA), followed by gel electrophoresis.
Assessment of HA-siRNA uptake by confocal microscopy

For the purpose of uptake studies, fluorescein-labeled scrambled siRNA was formulated with HA-PEI conjugated with rhodamine dye. Particles containing 10 nmol/L siRNA were incubated with SKOV-3WT and SKOV-3TR cells at 37 °C and cell uptake was assessed after 5, 15, or 30 minutes.

Transfection of siRNA against MDR-1 and PKM-2 to assess silencing of target mRNA expression

SKOV-3 cells were transfected with siRNA-loaded NPs (100 nmol/L siRNA) incubated for 72 or 96 hours. The cells were then harvested, and RNA was extracted and used to run quantitative PCR to assess mRNA levels. mRNA knockdown was determined by normalizing the expression of MDR-1 or PKM-2 to β-actin levels.

Cytotoxicity assay for single and combination siRNA therapy followed by paclitaxel

SKOV-3WT and SKOV-3TR cells were initially transfected with siMDR-1 and/or siPKM-2. After 72 hours, paclitaxel was added to assess the effect of cosensitization therapy. Cellular cytotoxicity was assessed by MTT assay 72 hours after paclitaxel treatment and expressed as the percentage of viable cells.

Establishment of subcutaneous SKOV-3WT tumors

Animal procedures were performed according to a protocol approved by Northeastern University, Institutional Animal Care and Use Committee (NI-IACUC). The tumor models for this study were developed in nude mice obtained from Charles River Laboratories (Wilmington, MA). Five- to 6-week-old nude mice were injected subcutaneously with SKOV-3WT tumor cells (5 × 105 cells + Matrigel) on the right flank. Tumor sizes were measured at least once or twice a week to monitor tumor growth.

Qualitative biodistribution studies of HA NPs using a near infrared (NIR)-encapsulated dye

The biodistribution of HA-PEI/PEG and dual-targeted HA NPs was assessed by encapsulating indocyanine green (ICG) into the NPs. Tumor-bearing mice were inoculated as described above, and the study commenced when the tumors reached an average size of ~200 mm3. The particles were then injected intravenously into mice bearing SKOV-3WT or SKOV-3TR tumors. Mice were imaged at 1, 2, 6, and 24 hours after the injection to monitor the distribution of the particles using an Xenogen IVIS Imaging System (Xenogen Corporation; Ex: 785 nm, Em: 820 nm).

Quantitative biodistribution and pharmacokinetic studies using siPKM-2 encapsulated in HA NPs

siRNA duplexes silencing PKM-2 was encapsulated in HA-PEI/HA-PEG NPs. These particles were injected into mice (n = 6/group) bearing ovarian tumors (SKOV-3WT) at 0.5 mg/kg twice a day on days 1, 3, and 5. Blood samples, major organs (liver, spleen, lung, heart, kidney), and tumors were collected 1, 6, or 24 hours following the last injection. The organs were then homogenized using Qiagen Tissue Lyser (Qiagen) to prepare tissue lysates. The homogenized tissue lysates were subsequently diluted 1:1,000, cDNA was generated, and qRT-PCR was performed. The PKM-2 siRNA sequence, reverse primer, forward primer, and an antiprimer sequence are listed below.

PKM-2 siRNA:

Sense: 5’-CCATIAACUGUCCUCACCAA-3’
Antisense: 5’-UUGGUGAGGACGAUUAUGG-3’
Primer:

Forward: /56-FAM/ACTCCCTTCCCTGATTTTTGGTGAGGAC-
Reverse: /785-BHQ1/GGAAGCCGACCCATAATCG

Antiprimer: AAATCAGGGGAGGGAG/3BHQ_1/

Evaluation of target gene knockdown in established subcutaneous SKOV-3 WT tumors

When subcutaneous tumors were ~150 and 200 mm3 in size, the animals were randomized into groups such that each group had similar tumor size. The animals were given an siRNA dose of 0.5 mg/kg twice a day on days 1, 3, and 5. Twenty-four after the last dose, the tumors were excised, RNA was extracted, and qRT-PCR was performed to determine the extent of MDR-1 and PKM-2 silencing.

Efficacy studies and toxicity analysis to determine safety of siRNA-encapsulated NPs in SKOV-3WT tumor-bearing mice

Animals bearing SKOV-3WT tumors were initially given an siRNA dose of 0.5 mg/kg twice a day every alternate days 1, 3, and 5. Paclitaxel was administered at a dose of 20 mg/kg once per week for 2 weeks. Tumor volumes were measured using the following formula to monitor the tumor growth inhibition: tumor volume = (length × width2)/2. The mice were weighed the day the treatments commenced and every day during the dosing period. To measure liver enzyme levels, blood was collected from all groups, and alanine aminotransferase (ALT)/aspartate aminotransferase (AST) levels were assessed. Liver, kidney, and spleen samples from mice were also collected for histopathological analysis at the end of the study.

In vivo–induced paclitaxel resistance development, efficacy studies, and safety analysis for combination therapy of siRNA with paclitaxel

For development of the in vivo–induced paclitaxel-resistant mouse model, the mice were inoculated subcutaneously with SKOV-3WT cells. When subcutaneous tumors were ~200 mm3 in size, the animals were treated with paclitaxel solution at a dose of 20 mg/kg every alternate day for 10 doses. One week...
following completion of paclitaxel therapy, the animals were randomized to different treatment groups, and tumor volume was measured to monitor for tumor growth inhibition. Body weight measurements were conducted throughout the entire period of efficacy studies. Liver, kidney, and spleen toxicity studies were conducted as described in section "Efficacy studies and toxicity analysis to determine safety of HA-encapsulated NPs."

Results

Formation of siRNA-loaded HA NPs determination of size, charge, morphology, siRNA encapsulation, and release by polyanion competition by gel retardation assay

Figure 1A provides a schematic representation of negatively charged siMDR-1/siPKM-2 encapsulation in HA-PEI/PEG particles. The self-assembling NPs showed a spherical morphology in TEM (Fig. 1B) with particles in the size range of 106 to 125 nm, polydispersity index (PDI) of 0.1 to 0.3, and surface charge in the range of −25 to −28 mV (Table 1). Electrophoretic retardation analysis of siRNA binding by HA-PEI with the release of intact siRNA by poly(acrylic acid). D, cell uptake studies in SKOV-3 WT and TR model. HA-rhodamine-123 and scramble siRNA labeled with fluorescein were incubated with the cells for 5, 15, and 30 minutes. The cells showed uptake within 15 minutes of incubation in the wild-type (WT) and resistant SKOV-3 cell lines. The dual-targeted system showed higher fluorescence signal compared with the HA-PEI/PEG system in both cell lines.

Transfection of MDR-1– and PKM-2–targeted siRNA to assess silencing of target gene expression

Transfection studies with siMDR-1 and siPKM-2 were conducted in SKOV-3WT (Fig. 2A) and SKOV-3TR cells (Fig. 2B) for 72 and 96 hours. Earlier and later time points were also assessed in preliminary studies, however, as these time points did not indicate a significant downregulation in gene expression these were not assessed further. Likewise, concentrations ranging from 50 and 200 nmol/L were assessed for activity. A concentration dependent downregulation of gene expression was observed and a concentration of 100 nmol/L was selected (lowest concentration with effective gene downregulation). Also, in our previous work with HA-PEI–based delivery systems we had observed, 100 nmol/L siRNA encapsulated in the HA-based systems provided effective downregulation with minimal cellular toxicity from PEI. Figure 2A measures the transfection efficiency of siMDR-1 and siPKM-2 in SKOV-3WT cells. A significant downregulation of MDR-1 was not observed even with Lipofectamine, as the basal levels of MDR-1 expression in the WT cells is fairly low; siPKM-2, however, showed an approximately 80% downregulation with Lipofectamine and both the NPs. Figure 2B reports the transfection efficiency of the delivery systems in SKOV-3TR cells. Both Lipofectamine and the NPs showed 80% to 85% gene expression downregulation with the NPs showing greater efficiency after longer periods of incubation compared with transfection achieved following use of Lipofectamine.

Cytotoxicity assay for single and combination siRNA therapy in combination with paclitaxel

Figure 2 shows the effect of single and combination therapy on paclitaxel IC50 in SKOV-3WT and SKOV-3TR cell lines. In SKOV-3WT cells, both the single and combination therapy did not show a significant change in paclitaxel IC50 values (P > 0.05). In SKOV-3TR cells, single therapy with siPKM-2 showed a significant decrease in paclitaxel IC50 values (P < 0.05). A 1.6-fold difference in the IC50 value was observed between siPKM2 encapsulated in dual-targeted NPs compared with HA-PEI/PEG NPs. Between single and combination therapy, combination therapy showed
a 1.3-fold decrease in IC$_{50}$ value ($P < 0.05$) compared with siMDR-1 therapy.

**Qualitative biodistribution studies using NIR-encapsulated dye in the HA nanoassemblies**

The whole body NP distribution in live animals was evaluated using an NIR dye, ICG encapsulated in HA NPs. ICG was loaded into HA-PEI/PEG NPs using a similar technique as used to encapsulate siRNA. These ICG loaded NPs had similar characteristics as siRNA encapsulated HA-PEI/PEG NPs (size range of ~200 nm, surface charge $-15$ mV). The ICG loaded NPs were intravenously injected in SKOV-3WT (Fig. 3A) and SKOV-3TR (Fig. 3B) tumor bearing mice at a dose equivalent to the dose used in efficacy studies. The NPs were stable during circulation following intravenous injection and the NIR signal was measured at different time points to capture the distribution pattern in live mice. Strong NIR signal was observed throughout the whole body 1 hour after administration with...
both the HA-PEI/PEG and dual-targeted NPs. A gradual decrease in signal intensity was observed over 6 hours with majority of the signal coming from liver and tumor regions 24 hours after ICG NP administration. Figure 3C shows ex vivo images of liver, kidney, spleen, heart, lungs, and tumors 24 hours after ICG administration. Among these tissues, liver showed the highest level of signal intensity, followed by the tumor, kidney, and spleen. We have previously observed that intravenous injection of free ICG in healthy mice shows a signal that is detectable in the liver as early as 3 minutes after injection, reaching a peak level between 5 and 10 minutes, indicative of a rapid hepatic clearance from the systemic circulation. The relatively short circulation time of free ICG could be attributed to fluorescence quenching of free ICG in physiological environments.

Quantitative biodistribution and pharmacokinetic studies using siPKM-2 encapsulated in HA nanoassemblies

After six intravenous injections of 0.5 mg/kg siRNA doses (in HA NP) into tumor bearing mice, blood and tissue samples were collected for siRNA quantitation at 1, 6, and 24 hours after last-administered dose. Accurate siRNA quantitation was studied using the antiprimer quenching based real-time PCR method. A fluorescently labeled PCR primer was designed to anneal to the template RNA and to a universal antiprimer. Following initial PCR, the temperature was lowered to allow the antiprimer to bind to unincorporated primer to quench the fluorescence. As double stranded PCR product would not bind with the antiprimer, an increase in fluorescent signal would enable siRNA quantitation. The siRNA was quantitated in each tissue and the % input dose per whole organ was calculated based on the starting siRNA.
dose. Figure 3D shows the biodistribution profile of siPKM-2 in HA-PEI/PEG NPs, whereas Fig. 3E indicates the distribution of the dual-targeted particles. With both the delivery systems, 30% to 40% of the siRNAs are detected in the liver, kidney, and spleen within 1 hour of administration. A very small proportion of the siRNA was detected in the plasma whereas 3% to 9% of the siPKM-2 was detected in the tumor tissues.

Evaluating target gene knockdown in SKOV-3 tumor-bearing mice

Figure 4A depicts in vivo gene downregulation following administration of siMDR-1 and siPKM2 in HA-PEI/PEG and the dual-targeted NPs. siMDR-1 delivery in SKOV-3WT tumor bearing mice showed a 20% downregulation of MDR-1 expression. A low level of endogenous MDR-1 expression in SKOV-3WT mice would be attributable to the lower degree of downregulation observed with siMDR1. With siPKM2 on the other hand, a 70% PKM2 downregulation was observed. Figure 4B shows in vivo gene downregulation following administration of the nano-assemblies in SKOV-3TR tumor bearing mice. The HA-PEI/PEG particles provided 40% MDR-1 downregulation and the dual-targeted NPs provided 65% MDR-1 downregulation. However, siPKM-2 HA-PEI/PEG and the dual-targeted NPs showed 60% to 70% down-regulation of gene expression.

Efficacy studies and toxicity analysis to determine safety of HA-encapsulated NPs

Figure 4C shows the effect of single and combination therapy of siRNA and paclitaxel in SKOV3WT tumor bearing mice. Tumor bearing mice were initially administered siMDR-1 and siPKM-2 as single or combination therapy twice a day every alternate day for 3 days. Twenty-four hours after the last dose, the animals were
In vivo paclitaxel resistance development, efficacy studies, and safety analysis for combination therapy of siRNA with paclitaxel

The in vivo paclitaxel resistance model was developed in SKOV-3WT tumor-bearing mice as described earlier. MDR-1/P-gp development was assessed using PCR and IHC. Figure 5A depicts the MDR-1 expression 1 and 3 weeks after paclitaxel administration. A 2- to 3-fold increase in MDR-1 expression was observed compared with control. P.KM-2 expression was unaltered in this model for the time period, which was assessed. IHC studies (Fig. 5B) confirmed this analysis where an increase in P-gp expression was observed compared with the PBS control group. Once development of resistance was confirmed, further SKOV-3WT tumor-bearing mice were recruited to a similar paclitaxel regimen to develop the in vivo resistance model. Following model development, the animals were randomized to the treatment groups and efficacy studies were conducted with the following treatment groups: PBS, NP with scramble siRNA, and dual-targeted NPs with siRNA as single therapy and combination therapy. Figure 5C shows the treatment efficacy following single and dual siRNA therapy with paclitaxel. All the treatment groups showed similar tumor volume measurements 2 weeks into therapy. However, 2 weeks after therapy, a difference in tumor volume was observed with combination of the two siRNA and paclitaxel showing the highest antitumor efficacy. Although therapy with a single siRNA did show reduced tumor volume growth compared with the control groups, there was a steady increase in tumor volume over the period of tumor assessment. In contrast with combination therapy, tumor volume sizes were maintained in the size range of 100 to 220 mm³. Table 3 indicates the TGI and TVD time. Single siRNA therapy showed 57% to 75% TGI (P < 0.05). However, only siPKM2-based therapy showed a significant increase in TVD when the siRNA were administered as single therapy. Combination therapy showed a significant increase in percentage TGI and an 8-fold (P < 0.05) increase in TVD time compared with the control group. Safety and toxicity analysis showed minimal effect on body weight, ALT, and AST levels.

Discussion

The aim of our current investigation was to study the effectiveness of combination therapy with siMDR-1 and siPKM-2 in SKOV-3WT and SKOV-3GR human ovarian adenocarcinoma cell lines and xenograft models. Previously, combination of MDR-1 gene silencing and chemotherapy administration has been assessed using polymeric NPs (11, 12, 19). These delivery systems have provided improved cytotoxicity attributed to an increased intracellular accumulation of anticancer agents upon MDR-1 gene silencing. Similarly, for PKM-2–based therapy, several nanocarrier-based delivery approaches have been reported in literature for anticancer activity. Goldberg and colleagues screened a library of siPKM-2 and identified a specific PKM-2 siRNA (si156), which when encapsulated in lipidoid NPs induced cell apoptosis showing tumor regression in HepG2 and SKOV3 xenograft tumor models (7). Another report showed that short hairpin RNA (shRNA) loaded in liposomal formulation showed effective PKM-2 silencing in human A549 lung cancer xenograft model and an increased efficacy in combination with cisplatin as an anticancer drug (10). PKM-2 silencing by shRNA loaded in Lipofectamine has also shown increased efficacy of docetaxel in a similar model. Thus, use of drug delivery systems to deliver anticancer drug (10). PKM-2 silencing by shRNA loaded in Lipofectamine has also shown increased efficacy of docetaxel in a similar model. Thus, use of drug delivery systems to deliver anticancer agents to cancer cells has been shown to have an increased efficacy. In this study, we wanted to extend the capability of our delivery system to assess the synergistic activity following the administration of combination of silRNA (targeting MDR-1 and PKM-2 expression) with paclitaxel in the treatment of ovarian cancer. As SKOV-3 cells have a high surface EGFR expression, we also examined the effect of actively targeted NPs in the delivery of these therapeutic agents (15). While testing these delivery systems in vivo, we explored the possibility of developing an in vivo paclitaxel resistance model, which would provide a realistic recapitulation of paclitaxel resistance development. Traditionally, in xenograft models paclitaxel resistance is developed by subcutaneous injection of cancer cells, which have been established by the reverse transformation technique, where the sublines are established in vitro by repeated or prolonged exposure to increasing doses of antineoplastic agents (23). However, these cells usually show strongly suppressed metastatic and/or tumorigenic properties in vivo, which makes

Table 2. Percentage tumor growth inhibition and tumor volume doubling time following treatment with single or combination therapy of siRNA and PTX in SKOV-3WT tumor-bearing mice

<table>
<thead>
<tr>
<th>Therapeutic groups</th>
<th>Tumor growth inhibition (%)</th>
<th>Tumor volume doubling time (days)</th>
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<tr>
<td>PBS</td>
<td>56</td>
<td>7.4 ± 4.8</td>
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<tr>
<td>PTX solution</td>
<td>56</td>
<td>10.9 ± 13.7</td>
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<tr>
<td>Naked siMDR1</td>
<td>9</td>
<td>7.7 ± 6.6</td>
</tr>
<tr>
<td>Naked siPKM2</td>
<td>5</td>
<td>7.6 ± 3.4</td>
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<tr>
<td>Scrambled HA-PEI/PEG NP</td>
<td>6</td>
<td>7.6 ± 6.5</td>
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<tr>
<td>Scrambled dual-targeted NP</td>
<td>12</td>
<td>7.8 ± 5.2</td>
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<td>NP-MDR1 HA-PEI/PEG NP</td>
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<td>NP-PKM2 HA-PEI/PEG NP</td>
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<td>NP-PKM2 dual-targeted NP</td>
<td>65</td>
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<td>NP-PKM2 + PKM2 HA-PEI/PEG NP</td>
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<tr>
<td>NP-PKM2 + PKM2 dual-targeted NP</td>
<td>82</td>
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Abbreviation: PTX, paclitaxel.

Injected with intravenous dose of paclitaxel at 20 mg/kg. This treatment regimen was repeated over 2 weeks and tumor volume measurements were measured every alternate day for 4 weeks. siRNA therapy in combination with paclitaxel showed significant improvement in efficacy. The siMDR-1 NPs showed a tumor growth profile similar to paclitaxel solution indicating that combination of siMDR-1 and paclitaxel has minimal effect on tumor growth. This effect could be correlated to low level of MDR1 expression in SKOV-3WT tumor bearing mice. Treatment with siPKM2 in both the NP systems showed slightly delayed tumor growth compared with paclitaxel solution (P > 0.05). Dual siRNA therapy showed a significant decrease in tumor volume compared with control animals. Table 2 shows the tumor growth time (TGI) and tumor volume doubling (TVD) time for all the treatment groups. Single siRNA therapy with paclitaxel showed 50% to 60% tumor inhibition (P < 0.05) compared with saline group. In comparison, combination therapy of dual siRNA and paclitaxel showed 72% to 84% tumor growth inhibition (P < 0.05). Similarly, this combination therapy group showed almost a 2-fold increase in tumor volume doubling time. Compared with paclitaxel solution, a significant increase in TGI and TVD time was not observed. Safety and toxicity analysis showed minimal effect on body weight, ALT, and AST levels (Supplementary Fig. S1).
them incompatible comparators to recurrent cancers, which show increased metastatic and/or tumor growth potential. Several groups have reported development of xenograft resistant models by administration of paclitaxel in a subcutaneous model followed by excision and retransplantation over 6 months and the final tumor-derived cells being established and maintained as in vivo resistance sublines (24). In this study, we aimed to develop in vivo paclitaxel resistance by repeated administration of paclitaxel to recapitulate clinical resistance development and assess the effectiveness of our therapies in these models.

The siRNA nano-assemblies were prepared by charged based encapsulation of siRNA into HA-PEI particles. HA is a naturally occurring mucopolysaccharide composed of alternating disaccharide units of D-glucuronic acid and N-acetyl-D-glucosamine (NAG) with $\beta (1 \rightarrow 4)$ interglycosidic linkage. It is a highly anionic biopolymer present in the extracellular matrix and synovial fluids. It is biodegradable, nontoxic, nonimmunogenic and noninflammatory, which makes it an ideal carrier polymer for systemic drug delivery applications. The HA backbone specifically recognizes CD44, an integral membrane glycoprotein overexpressed on several tumor cell surfaces including tumor-initiating stem cells. Similarly, PEI is widely used for nucleic acid delivery, including siRNA delivery where nucleic acids are condensed by electrostatic interactions to form dense particles (complexes), which protect the genetic material from enzymatic degradation and promote

Table 3. Percentage tumor growth inhibition and tumor volume doubling time following treatment with single or combination therapy of siRNA and PTX in SKOV-3TR tumor-bearing mice

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<th>Tumor volume doubling time (days)</th>
</tr>
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<tr>
<td>PBS</td>
<td>10.7 ± 8.6</td>
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<tr>
<td>PTX solution</td>
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<tr>
<td>NP-MDR1 + PKM2 dual-targeted NP</td>
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Abbreviation: PTX, paclitaxel.

Figure 5. In vivo paclitaxel (PTX) resistance model development: A, qPCR studies to assess MDR-1 and PKM-2 expression; B, immunofluorescence of tumor tissues from P-gp and PKM-2 expression in PBS-treated and PTX-treated animals. C, schematic representation of the dosing schedule adopted to develop the SKOV-3TR mouse model followed by NP treatment. D, effect of the combination of paclitaxel treatment and MDR1 and PKM2 silencing on growth of SKOV3TR tumors.

The siRNA nano-assemblies were prepared by charged based encapsulation of siRNA into HA-PEI particles. HA is a naturally occurring mucopolysaccharide composed of alternating disaccharide units of D-glucuronic acid and N-acetyl-D-glucosamine (NAG) with $\beta (1 \rightarrow 4)$ interglycosidic linkage. It is a highly anionic biopolymer present in the extracellular matrix and synovial fluids. It is biodegradable, nontoxic, nonimmunogenic and noninflammatory, which makes it an ideal carrier polymer for systemic drug delivery applications. The HA backbone specifically recognizes CD44, an integral membrane glycoprotein overexpressed on several tumor cell surfaces including tumor-initiating stem cells. Similarly, PEI is widely used for nucleic acid delivery, including siRNA delivery where nucleic acids are condensed by electrostatic interactions to form dense particles (complexes), which protect the genetic material from enzymatic degradation and promote
their cellular uptake by absorptive endocytosis. PEI also has an intrinsic endosomal escape mechanism known as the 'proton sponge' effect, which causes osmotic swelling and rupture of the endosome membrane, triggering the release of PEI complexes into the cytosol. In this study, for the preparation of the complexes, a 54:1 polymer:sirNA ratio was adapted from our previous studies, where optimal encapsulation and release was observed with this ratio (21). At these ratios, we obtained ~92% to 95% encapsulation efficiency of siRNA. Similarly, for in vitro studies, we selected a siRNA concentration of 100 nmol/L because of effect of higher concentrations on cell viability (Supplementary Fig. S2). For the incorporation of EGFR-targeted HA, in our preliminary investigation, we altered the ratio of HA-EGF and determined the transfection efficiency (Supplementary Fig. S3). Earlier transfection periods showed increased downregulation of gene expression; however, at later time points, altering ratios did not have a significant effect on downregulation of MDR-1 expression.

Following the preparation of these particles uptake and transfection, studies showed efficient uptake and transfection with both the NP systems showing similar decrease in gene expression in both SKOV-3WT and SKOV-3TR cell lines. Synergistic activity of dual siRNA therapy showed minimal effect on SKOV-3WT but had a significant effect on IC50 of paclitaxel in SKOV-3TR cell lines. In SKOV-3WT cells, as there is a low level of basal MDR-1, the cells would be sensitive to paclitaxel thus HA-siMDR-1 expression would have minimal effect on cytotoxicity. In contrast, SKOV-3TR cells have an increased MDR-1 expression; thus, single therapy with siMDR-1 would affect cytotoxicity. Additionally, combination therapy with siMDR-1 and siPKM-2 showed a further improvement in cytotoxicity, which could be attributed to synergistic effect of siMDR-1 on P-gp expression and PKM-2 on the glycolytic pathway. A minimal effect on cytotoxicity was observed with both the NP delivery systems, which could be attributed to similar uptake profile of these delivery systems in vitro.

In vivo biodistribution studies indicated a high degree of accumulation of the NPs in the liver, kidney, and spleen because of preferential uptake of these particles by macrophages residing in these tissues. Although a small proportion of the total siRNA dose was detected at the tumor site, in vivo knockdown studies showed a significant downregulation of gene expression. This downregulation translated to a small improvement in antitumor efficacy following combination therapy of dual siRNA and paclitaxel with minimal toxicity.

After in vivo studies in SKOV-3WT tumor bearing models, the efficacy of the delivery systems was assessed in the in vivo paclitaxel resistant model. This model was developed over 6 weeks of therapy and MDR-1 expression was determined. As a significant difference in an increase in MDR-1 expression was not observed between 4 and 6 weeks after paclitaxel treatment, we initiated in vivo studies in TR model within 4 weeks of therapy. Post-model development and dosing with NP with a similar regimen as was adopted in the WT model there was an improvement in antitumor efficacy with siRNA-based therapy. Dual siRNA-based approach further augmented the antitumor effect possibly because of synergistic effect of siMDR-1 on P-gp expression, leading to increased cellular paclitaxel concentration and the effect of siPKM-2 on the glycolysis pathway affecting cancer cell metabolism. Thus, combination of siRNA with cytotoxic agents provided synergistic effect and enhanced antitumor efficacy because of its actions on different resistance mechanisms in cancer.

Conclusions

In summary, anticancer therapeutics employing RNAi mechanism holds promise for sequence-specific silencing of target genes. However, targeted delivery to tumor sites remains a major hurdle for cancer therapy. Thus, in this study, we evaluated encapsulation and delivery of siMDR-1 and siPKM-2 in HA-PEI–based self-assembling nanosystems for the treatment of WT and resistant ovarian cancer. The nano-assemblies showed effective transfection and improved cytotoxic effect of paclitaxel in cancer cells. Although the effect was not pronounced in WT animal models, dual therapy provided action of these therapeutic agents on multiple pathways in cancer cells providing synergistic activity for cancer therapy. Although an in vivo paclitaxel resistance model was developed to assess the effectiveness of our therapies, future studies in paclitaxel resistance model development in orthotopic or genetically modified ovarian cancer mice would indicate further clinical relevance of these therapies.

Disclosure of Potential Conflicts of Interest

No potential conflicts of interest were disclosed.

Authors' Contributions

Conception and design: M. Talekar, M.S. Goldberg, M.M. Amiji
Development of methodology: M. Talekar
Acquisition of data (provided animals, acquired and managed patients, provided facilities, etc.): M. Talekar
Analysis and interpretation of data (e.g., statistical analysis, biostatistics, computational analysis): M. Talekar, Q. Ouyang
Writing, review, and/or revision of the manuscript: M. Talekar, Q. Ouyang, M.S. Goldberg, M.M. Amiji
Administrative, technical, or material support (i.e., reporting or organizing data, constructing databases): M. Talekar
Study supervision: M. Talekar, M.S. Goldberg, M.M. Amiji

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Cosilencing PKM-2 and MDR-1 in Ovarian Cancer


Cosilencing of PKM-2 and MDR-1 Sensitizes Multidrug-Resistant Ovarian Cancer Cells to Paclitaxel in a Murine Model of Ovarian Cancer

Meghna Talekar, Qijun Ouyang, Michael S. Goldberg, et al.

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